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SYSTEM:OS  - DIALOG OneSearch
  File 155:MEDLINE(R) 1951-2005/Jan W1
         (c) format only 2005 The Dialog Corp.
*File 155: Medline has resumed updating. Please see
HELP NEWS 155 for details.
  File   2:INSPEC 1969-2005/Dec W3
         (c) 2005 Institution of Electrical Engineers
*File   2: Price change effective Jan 1, 2005. Enter HELP
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  File   5:Biosis Previews(R) 1969-2005/Dec W4
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*File  73: Price change effective Jan 1, 2005. Enter HELP
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  File  94:JICST-EPlus 1985-2005/Dec W1
         (c)2005 Japan Science and Tech Corp(JST)
  File  35:Dissertation Abs Online 1861-2004/Dec
         (c) 2004 ProQuest Info&Learning
  File 144:Pascal 1973-2004/Dec W1
         (c) 2004 INIST/CNRS
*File 144: Price change effective Jan 1, 2005. Enter HELP
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         (c) 2001 Australian Mineral Foundation Inc
*File 105: This file is closed (no updates)
  File  99:Wilson Appl. Sci & Tech Abs 1983-2004/Nov
         (c) 2004 The HW Wilson Co.
  File  58:GeoArchive 1974-2004/Oct
         (c) 2004 Geosystems
  File  34:SciSearch(R) Cited Ref Sci 1990-2005/Jan W2
         (c) 2005 Inst for Sci Info
*File  34: Price change effective Jan 1, 2005. Enter HELP
RATES 34 for details.
  File 434:SciSearch(R) Cited Ref Sci 1974-1989/Dec
         (c) 1998 Inst for Sci Info
*File 434: Price change effective Jan 1, 2005. Enter HELP
RATES 434 for details.
  File 292:GEOBASE(TM) 1980-2004/Dec B1
         (c) 2004 Elsevier Science Ltd.
*File 292: Price change effective Jan 1, 2005. Enter HELP
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  File  89:GeoRef 1785-2005/Dec B2
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*File 89: Please see HELP ALERTALL for new Alert frequency and price. Please see HELP RATES 89 for new Academic Subscriber rates.
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File 350:Derwent WPIX 1963-2005/UD,UM &UP=200503
(c) 2005 Thomson Derwent
*File 350: For more current information, include File 331 in your search. Enter HELP NEWS 331 for details.
File 347:JAPIO Nov 1976-2004/Aug(Updated 041203)
(c) 2004 JPO & JAPIO
*File 347: JAPIO data problems with year 2000 records are now fixed. Alerts have been run. See HELP NEWS 347 for details.

Set	Items	Description
S1	781	AU=(DIETZ, P? OR DIETZ P?)
S2	18	AU=(KIMMLINGEN, R? OR KIMMLINGEN R?)
S3	796	S1:S2
S4	34	S3 AND (MRI OR MAGNETIC(1W)(IMAG? OR IMAGING) OR MAGNETIC(-W)RESONAN? OR NMR OR NUCLEAR()MAGNETIC()RESONANCE OR FTNMR OR FTMRI OR MAGNETORESONANCE OR PMR OR PROTON(W)MAGNETIC(W)RESONAN? OR MR()(IMAGE? OR IMAGING))
S5	0	S4 AND (MAGNET? OR RESONANC?)(3N)SCANNER? ?
S6	2	S4 AND EDDY(2N)CURRENT? ?
S7	2	RD (unique items)
S8	32	S4 NOT S6
S9	29	RD (unique items)
S10	9	S9 AND GRADIENT?(3N)FIELD? ?
S11	9	RD (unique items)
S12	1788024	MRI OR MAGNETIC(1W)(IMAG? OR IMAGING) OR MAGNETIC(W)RESONAN? OR NMR OR NUCLEAR()MAGNETIC()RESONANCE OR FTNMR OR FTMRI OR MAGNETORESONANCE OR PMR OR PROTON(W)MAGNETIC(W)RESONAN? OR MR()(IMAGE? OR IMAGING)
S13	41805	MC=(S01-E02A2 OR S03-E07A OR S01-E02A8A OR S01-E02A1 OR S03-E07C OR S05-D02B1 OR S03-C02F1) OR IC=(G01R-003 OR G01N-024/08 OR G01V-003/A75) OR CC=(A0758 OR A8760I OR B7510N)
S14	796	S1:S2
S15	3241	(MAGNET? OR RESONANC?)(3N)SCANNER? ?
S16	65015	EDDY(2N)CURRENT? ?
S17	54918	GRADIENT?(3N)FIELD? ?
S18	454368	CONDUCT?(3N)ELECTRICAL?
S19	320070	(FIRST OR ONE OR TWO OR SECOND OR THREE OR THIRD)(3N)CONDUCT?
S20	14384	CONDUCT?(2N)SECTION? ?
S21	332201	S19:S20
S22	835451	COMPENSAT?
S23	44881	(COIL? ? OR SPIRAL???? OR CONCENTRIC????? OR WIRE????)(3N)ARRANGE? ?
S24	1802136	S12:S13
S25	2351	S24 AND S15
S26	20	S25 AND S16
S27	17	RD (unique items)
S28	2331	S25 NOT S26
S29	47	S28 AND S17
S30	1	S29 AND S18
S31	46	S29 NOT S30
S32	0	S31 AND S21
S33	2	S31 AND S22
S34	2	RD (unique items)
S35	44	S31 NOT S33
S36	0	S35 AND S23
S37	0	S35 AND S19
S38	30	RD S35 (unique items)
S39	605	S23 AND S22
S40	1	S39 AND S20
S41	91	S23 AND S20
S42	6	S41 AND S16
S43	6	RD (unique items)
S44	85	S41 NOT S42
S45	1	S44 AND S17

S46	84	S44 NOT S45
S47	0	S46 AND S15
S48	7	S46 AND S24
S49	7	RD (unique items)

Query/Command : HIS

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File : PLUSPAT

SS  Results
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  2          3  (1) ..FAM US20040222795/PN
  3          1  ..CITF US20040222795/PN
  4          1  ..CITB US20040222795/PN

Search statement   5
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Query/Command : PRT MAX SET

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1 / 1 PLUSPAT - ©QUESTEL-ORBIT - image

PN - US2004222795 A1 20041111 [US20040222795]

TI - (A1) Magnetic resonance apparatus with eddy current compensation

IN - (A1) DIETZ PETER (DE); KIMMLINGEN RALPH (DE)

AP - US77755404 20040212 [2004US-0777554]

PR - DE10305835 20030212 [2003DE-1005835]
DE102004004293 20040128 [2004DE-10004293]

IC - (A1) G01V-003/00

EC - G01R-033/385

PCL - ORIGINAL (O) : 324318000; CROSS-REFERENCE (X) : 324322000

DT - Corresponding document

STG - (A1) Utility Patent Application published on or after January 2, 2001

AB - A magnetic resonance apparatus has a coil arrangement to generate a magnetic gradient field in an imaging volume and an electrically-conductive structure that at least partially surrounds the coil arrangement and in which, given a temporally changing current flow in the coil arrangement, eddy currents are caused that produce an eddy current field interfering with the gradient field within the imaging volume. For eddy current compensation the coil arrangement has at least two conductor sections from the group of: a first conductor section that contributes to the generation of the gradient field, and that additionally generates via the electrically-conductive structure a first interference factor in the form of a first eddy current field in the imaging volume, a second conductor section that contributes both to the generation of the gradient field, thereby generating via the electrically-conductive structure a second interference factor in the form of a second eddy current field in the imaging volume, and that generates a field compensating the first eddy current field, and a third conductor section that contributes exclusively to the compensation of interference factors in the form of an eddy current field. One of the conductor sections contributing to the compensation of interference factors is spaced, relative to the imaging volume, at less than or equal to the distance of one of the conductor sections contributing to the gradient field.

UP - 2004-46

Search statement 2

Query/Command : PRT MAX SET

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PN - US2004222795 A1 20041111 [US20040222795]

TI - (A1) Magnetic resonance apparatus with eddy current compensation

IN - (A1) DIETZ PETER (DE); KIMMLINGEN RALPH (DE)

AP - US77755404 20040212 [2004US-0777554]

PR - DE10305835 20030212 [2003DE-1005835]
DE102004004293 20040128 [2004DE-10004293]

IC - (A1) G01V-003/00

EC - G01R-033/385

PCL - ORIGINAL (O) : 324318000; CROSS-REFERENCE (X) : 324322000

DT - Corresponding document

STG - (A1) Utility Patent Application published on or after January 2, 2001

AB - A magnetic resonance apparatus has a coil arrangement to generate a magnetic gradient field in an imaging volume and an electrically-conductive structure that at least partially surrounds the coil arrangement and in which, given a temporally changing current flow in the coil arrangement, eddy currents are caused that produce an eddy current field interfering with the gradient field within the imaging volume. For eddy current compensation the coil arrangement has at least two conductor sections from the group of: a first conductor section that contributes to the generation of the gradient field, and that additionally generates via the electrically-conductive structure a first interference factor in the form of a first eddy current field in the imaging volume, a second conductor section that contributes both to the generation of the gradient field, thereby generating via the electrically-conductive structure a second interference factor in the form of a second eddy current field in the imaging volume, and that generates a field compensating the first eddy current field, and a third conductor section that contributes exclusively to the compensation of interference factors in the form of an eddy current field. One of the conductor sections contributing to the compensation of interference factors is spaced, relative to the imaging volume, at less than or equal to the distance of one of the conductor sections contributing to the gradient field.

UP - 2004-46

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2 / 3 PLUSPAT - ©QUESTEL-ORBIT

PN - DE102004004293 A1 20040909 [DE102004004293]

OTI - (A1) Magnetresonanzgerät mit einer Spulenanordnung und einer elektrisch leitfähigen Struktur

PA - (A1) SIEMENS AG (DE)

IN - (A1) DIETZ PETER (DE); KIMMLINGEN RALPH (DE)

AP - DE102004004293 20040128 [2004DE-10004293]
PR - DE102004004293 20040128 [2004DE-10004293]
DE10305835 20030212 [2003DE-1005835]
IC - (A1) G01R-033/385 G01R-033/421
EC - G01R-033/385
DT - Basic
STG - (A1) Doc. Laid open (First publication)
UP - 2004-37

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3 / 3 PLUSPAT - ©QUESTEL-ORBIT

PN - GB0403161 D0 20040317 [GB200403161]
PN2 - GB2400671 A 20041020 [GB2400671]
TI - (D0) Magnetic resonance apparatus with a coil arrangement and an electrically conducting structure
PA - (D0) SIEMENS AG
PA2 - (A) SIEMENS AG (DE)
IN - (A) DIETZ PETER (DE); KIMMLINGEN RALPH (DE)
AP - GB0403161 20040212 [2004GB-0003161]
PR - DE10305835 20030212 [2003DE-1005835]
DE102004004293 20040128 [2004DE-10004293]
IC - (A) G01R-033/385 G01R-033/3875
EC - G01R-033/385
DT - Corresponding document
CT - Cited in the search report
EP164199(A1);EP304126(A1);JP2002112977(A)
STG - (D0) Application for patent
STG2 - (A) Application published
AB - To compensate for eddy currents 11 produced in vacuum tank 10 the gradient coil assembly comprises conductor sections controllable at least partially independently of each other so that some conductors can additionally or exclusively compensate for eddy currents. For example in Fig 1,3 conductor sections 111,112,113 contributes to generating the gradient field, additionally generating a first eddy current field in the imaging volume, conductor section 121,122 which contributes to generating the gradient field, thus generating a second eddy current field in the imaging volume, also generates fields compensating the eddy current field produced from conductors 112,113. A third conductor section 131 compensates exclusively for eddy current fields produced from other conductors. The arrangement is such that the conductor sections contributing to compensating eddy currents is at a smaller or identical distance from the imaging volume than one of the conductor sections contributing to the gradient field. In an alternative embodiment fig 5 conductor sections 130 act as compensating coil. Control

maybe by separate supplies 31-33, a single supply 50 and a switch 55 or a common supply associated with filters and inductive transformers (fig 4).n

UP - 2004-15

Search statement 3